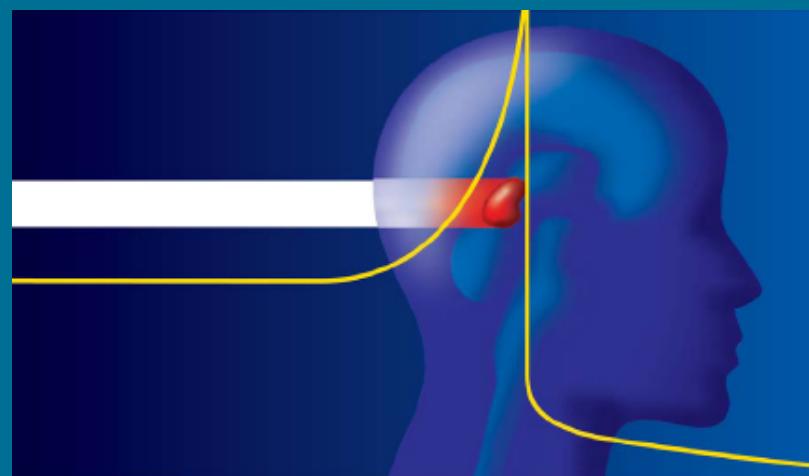


Autumn Lectures / Tbilisi / 2013

Tumor therapy with protons and light ions

21 October 2013 | Markus Büscher

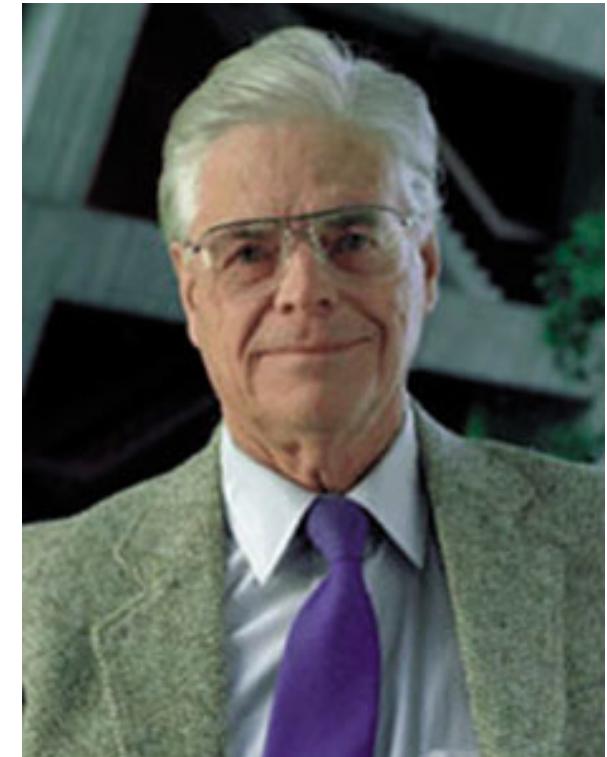


Proton Beam Therapy – History

A Man - A Vision

In 1946 Harvard physicist
Robert Wilson (1914-2000) suggested*:

- **Protons can be used clinically**
- **Accelerators are available**
- **Maximum radiation dose can be placed into the tumor**
- **Proton therapy provides sparing of normal tissues**
- **Modulator wheels can spread narrow Bragg peak**



Proton Beam Therapy – History

- 1946 R. Wilson suggests use of protons
- 1954 First treatment of pituitary tumors
- 1958 First use of protons as a neurosurgical tool
- 1967 First large-field proton treatments in Sweden
- 1974 Large-field fractionated proton treatments program begins at HCL, Cambridge, MA
- 1990 First hospital-based proton treatment center opens at Loma Linda University Medical Center

Proton Beam Therapy – Today

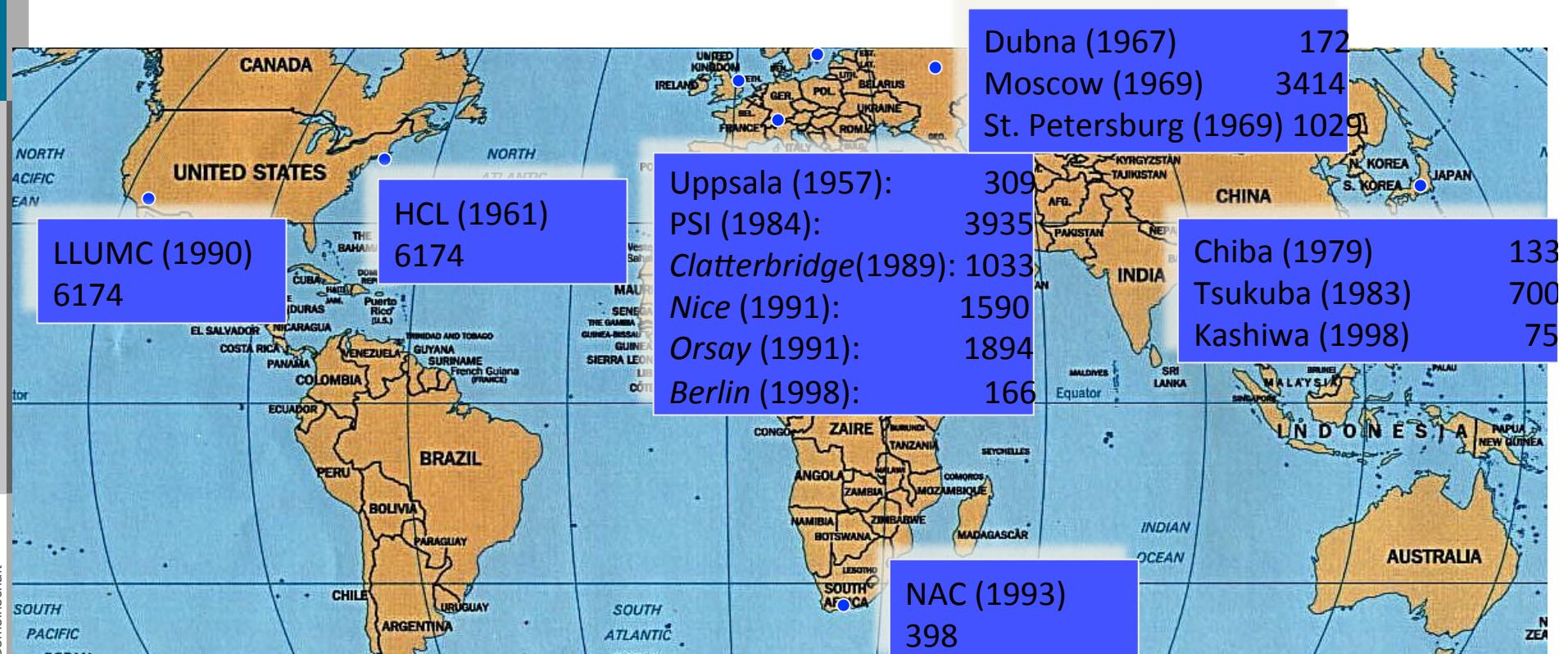
X-ray and Proton therapy are well established

Protons:

- 5,000 – 10,000 potential patients p.a. in Germany

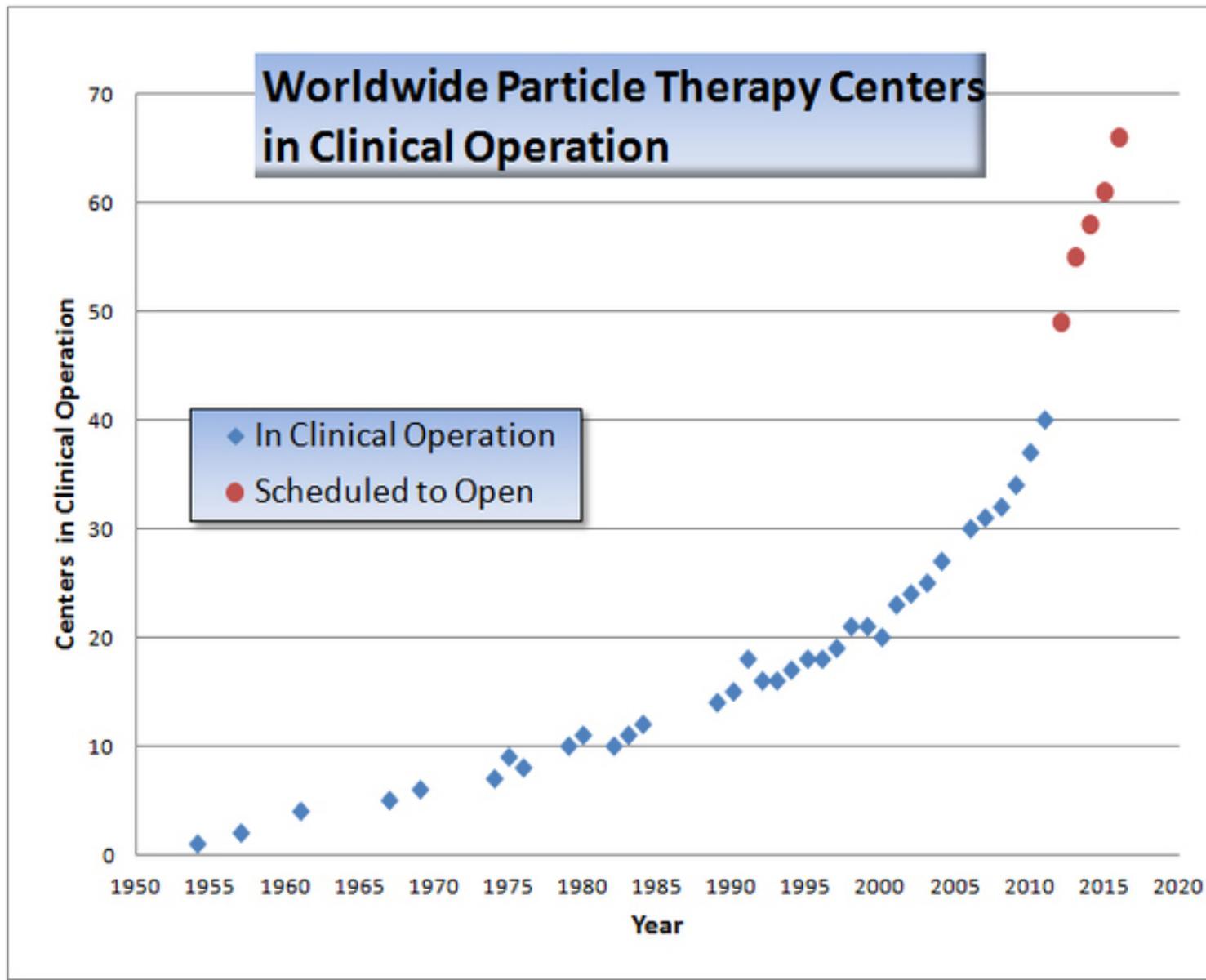
Proton Beam Therapy – Today

World wide: 39 therapy centers / 55.000 treatments p.a.



Next generation: Carbon ions

Proton Beam Therapy – Today

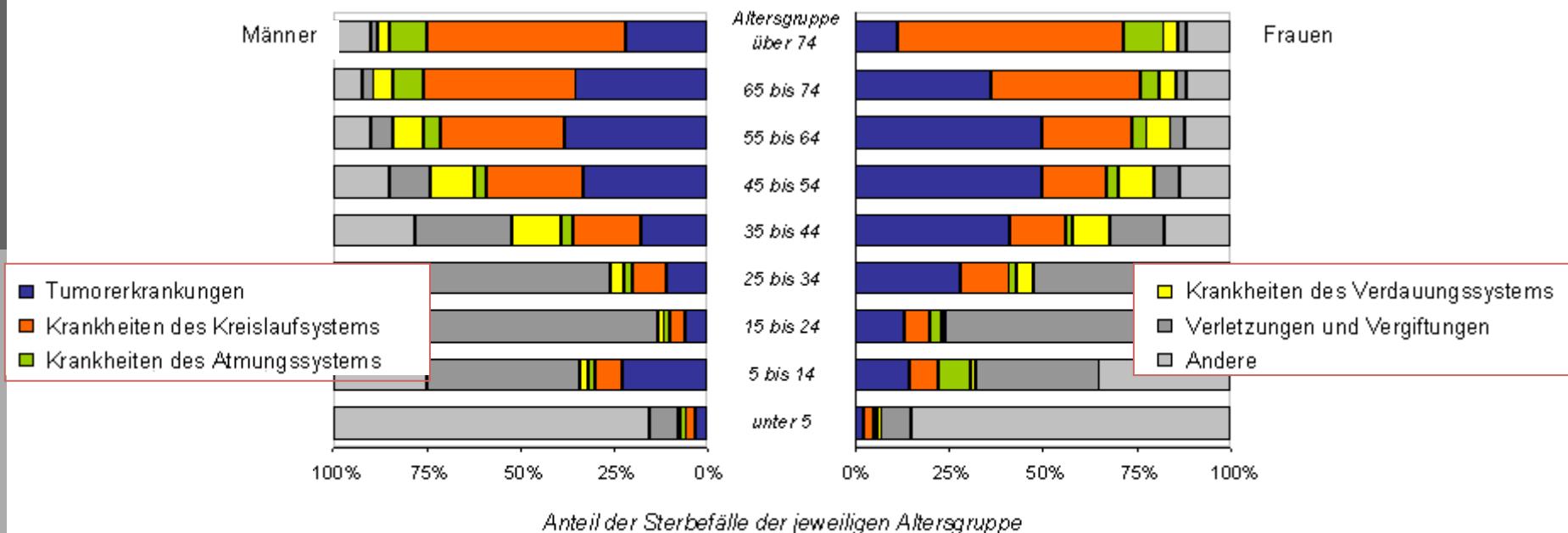


Proton Beam Therapy – Cancer

~486,000 incidences per year in Germany

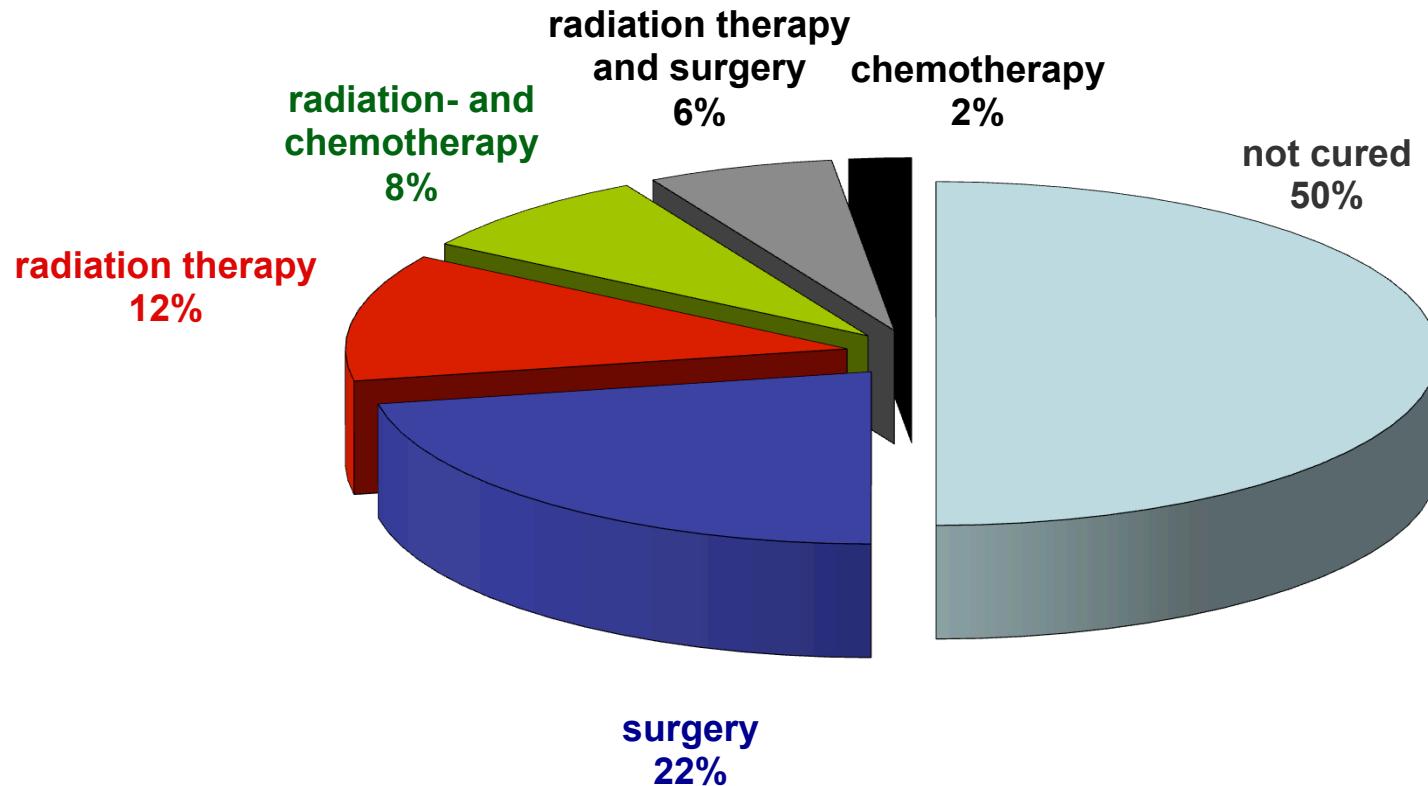
Every 3rd human gets a malignancy during her/his lifetime

Every 5th person dies of cancer

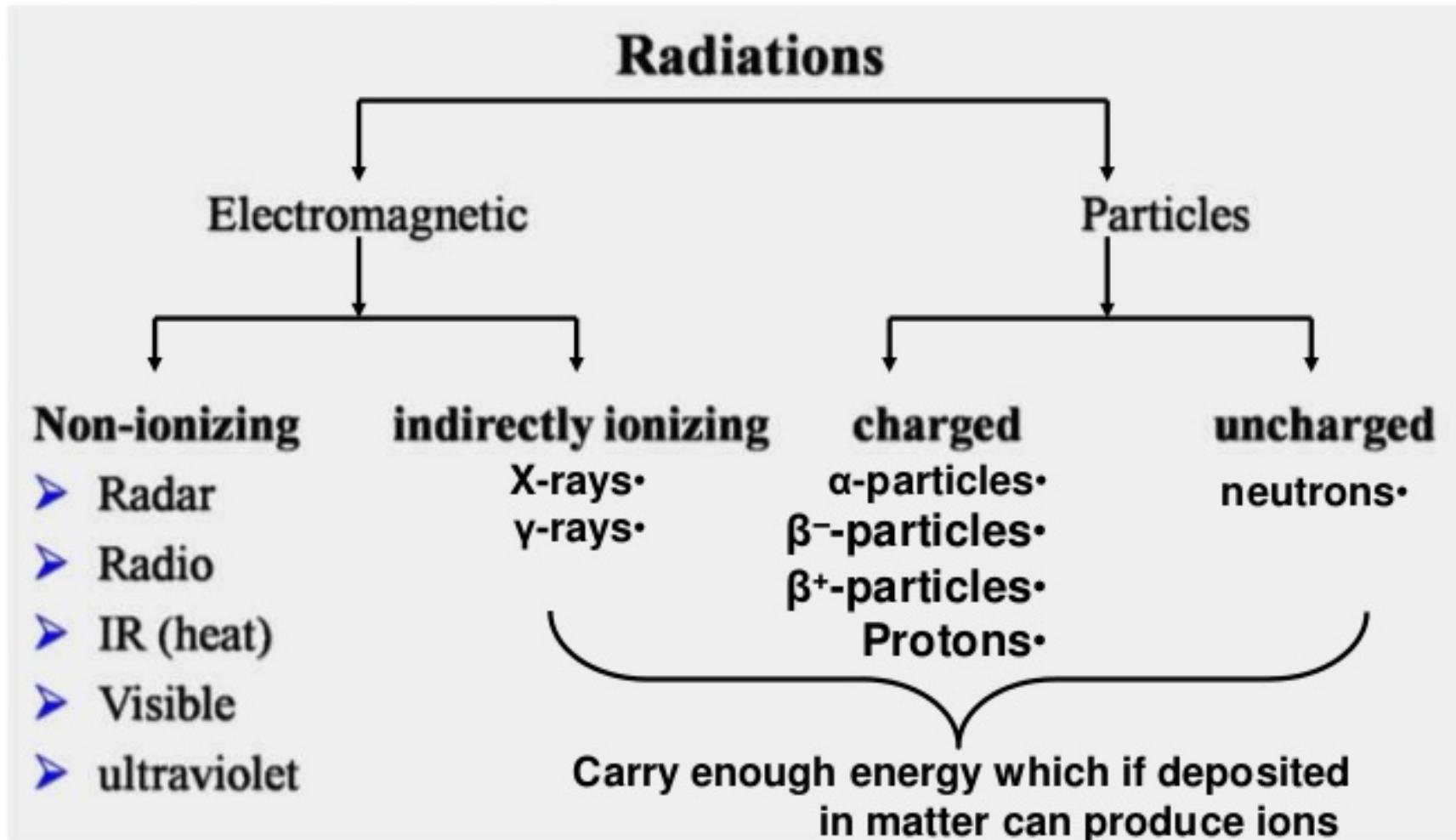


Proton Beam Therapy – Cancer

Treatments



taken from: Cancer Statistics Review, NIH 1992



Proton Beam Therapy – Radiation

X rays: discovery 1895



Wilhelm Conrad Röntgen 1845 – 1923
Nobel price for physics 1901

First x-ray picture:
Mrs. Röntgen's hand



X rays interact with human tissue!

First successful treatment: 1899 (skin cancer)

Proton Beam Therapy – Radiation

X rays: interaction with matter

Photo effect

Incident Photon

Photo electron

Compton scattering

Incident Photon

Scattered photon

Pair creation

Incident Photon

x-ray photon is absorbed, resulting in the ejection of electrons from the outer shell

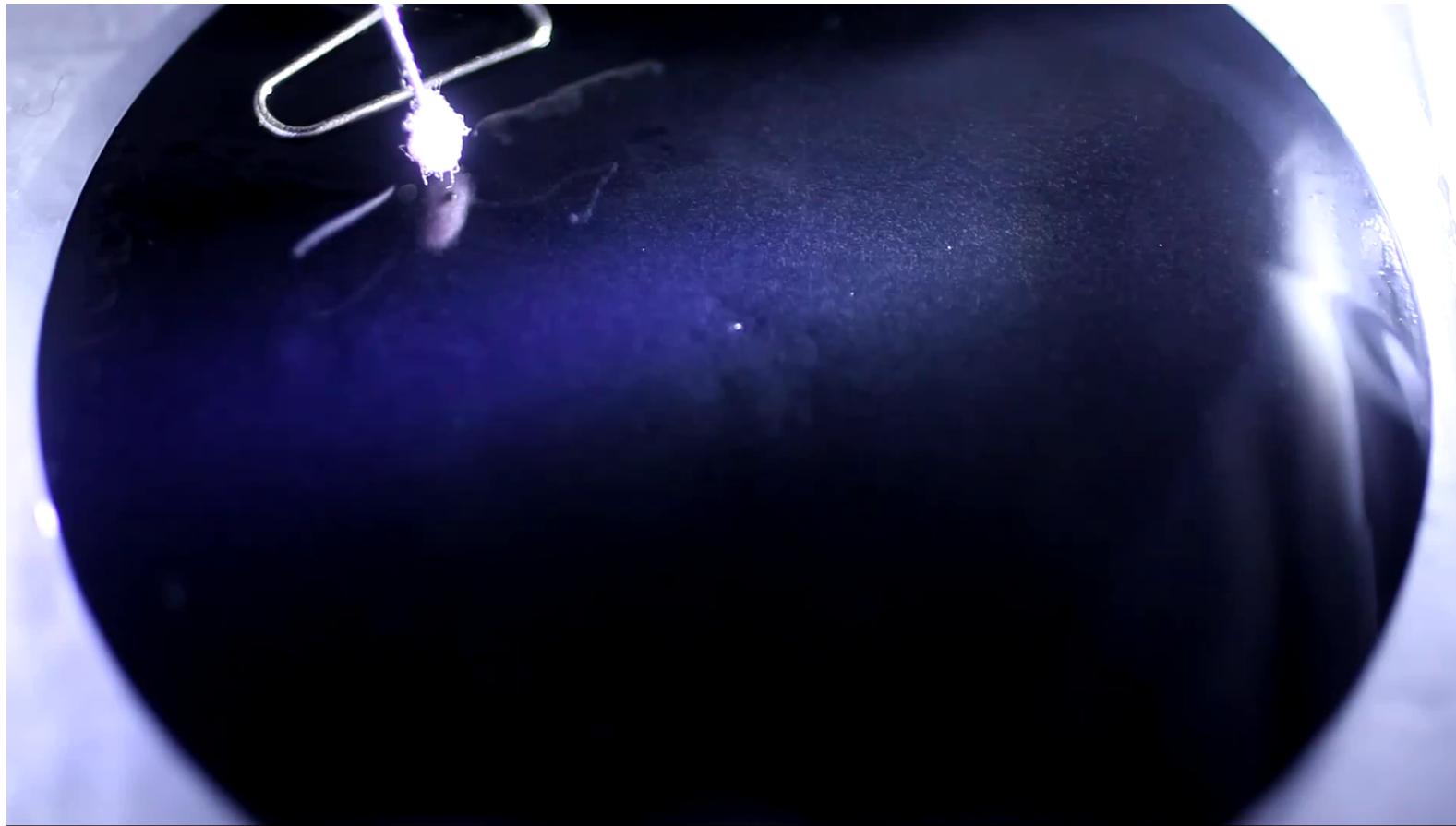
x-ray photon is deflected by an interaction with an electron. The electron gains energy and is ejected from its orbital position

electron and positron pair is created with the annihilation of the x-ray photon

→ Full energy deposit close to the point of absorption

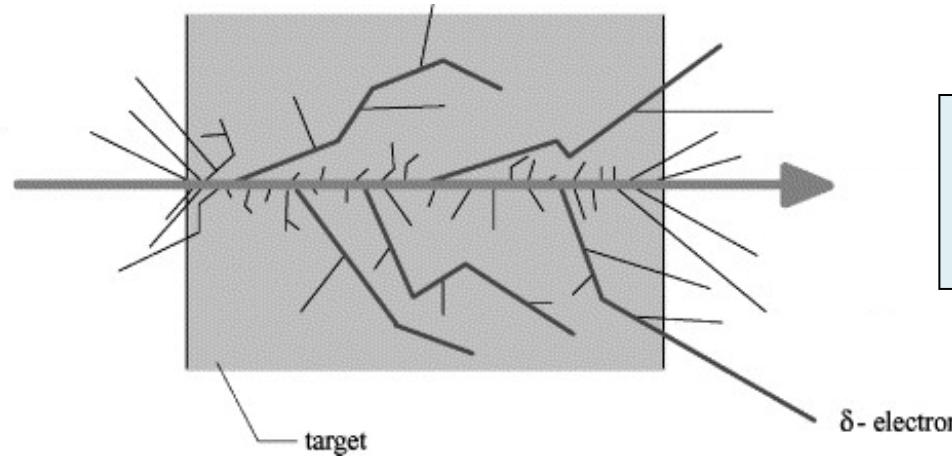
Proton Beam Therapy – Radiation

Charged particles: continuous energy loss / tracks



Proton Beam Therapy – Radiation

Charged particles: continuous energy loss

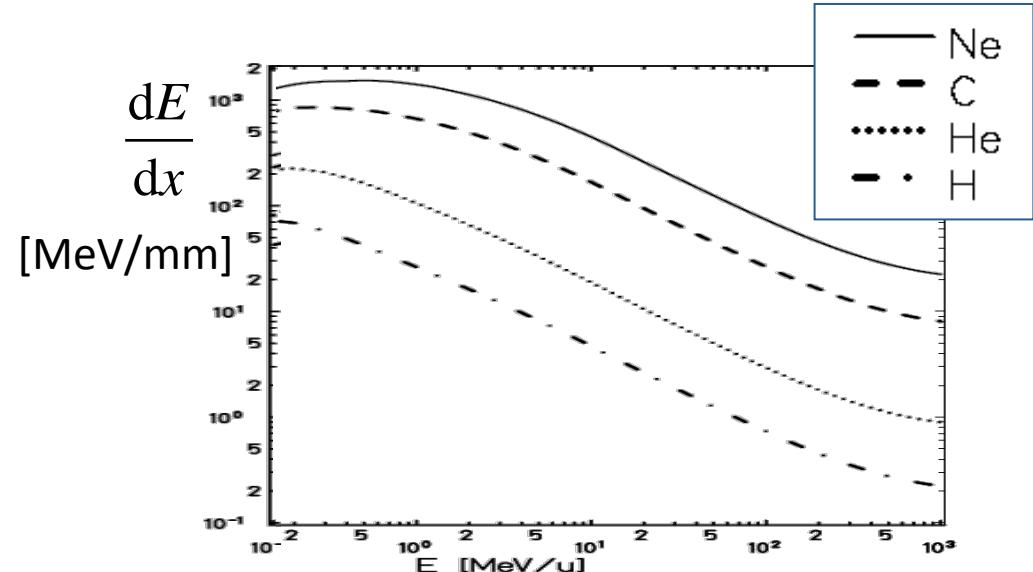


Energy loss through
production of
 δ elektrons (ionization)

Bethe-Bloch formula

$$-\frac{dE}{dx} = \frac{4\pi e^4 N_a Z z_{eff}^2}{m_e v^2} \ln \frac{2mv^2}{I}$$

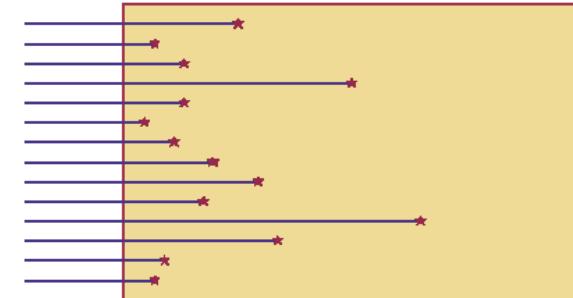
+ relativistic terms



Photons

It cannot be predicted where a certain photon is absorbed

Energy is deposited close to the point of the first interaction

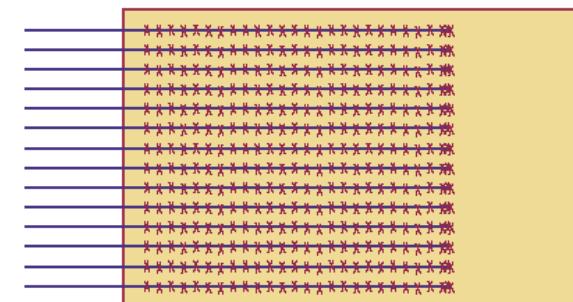


Penetration depth x

Charged particles

Continuous energy loss

Well defined range



→Which one is better for radiation therapy?
(energy deposit as function of penetration depth?)

The essentials of radiation therapy:

Biological effect of radiation mediated by ionization

Photons Charged particles

Higher ionization density ($\rightarrow dN/dx, dE/dx$) means that more tumor cells are killed

Tumors can tolerate (at least) as much radiation as healthy tissue.
Dose must be localized to the tumor!

Proton Beam Therapy – Energy deposit

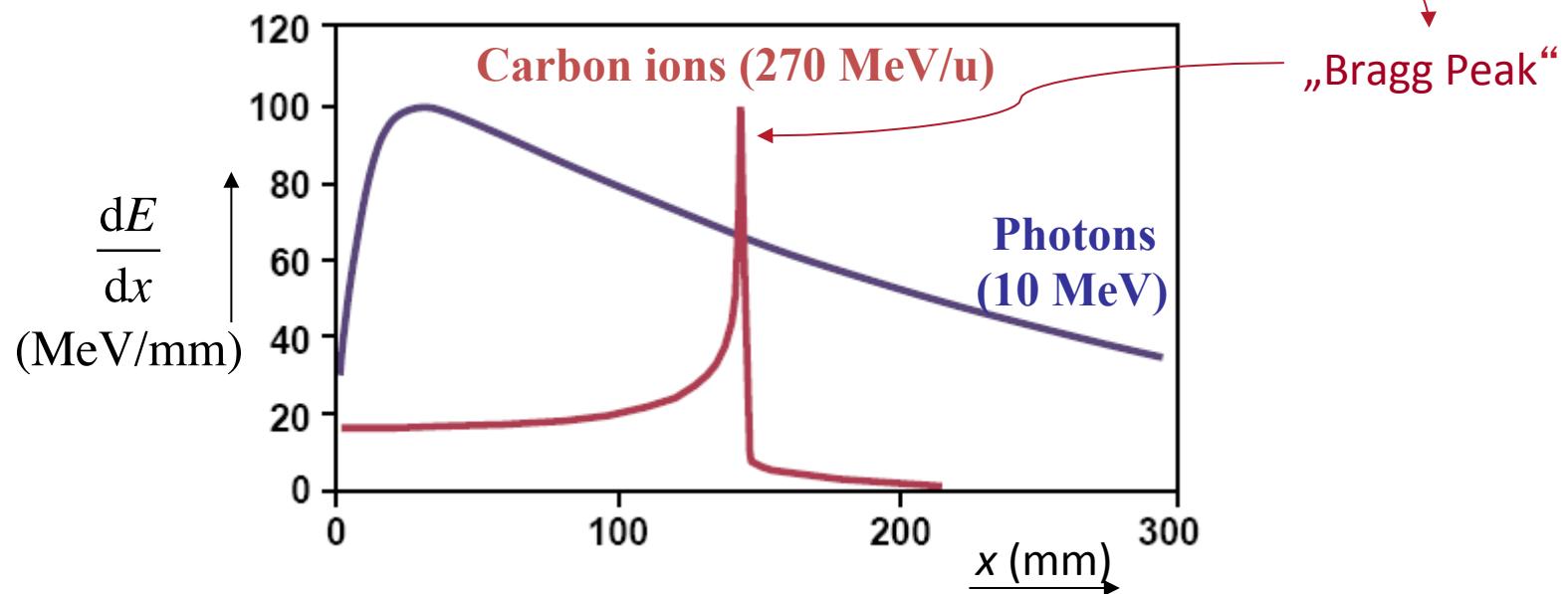
Photons:

$$-\frac{dN(x)}{dx} \propto N(x) \Rightarrow \frac{dN(x)}{dx} \propto e^{-x}$$

Charged particles:

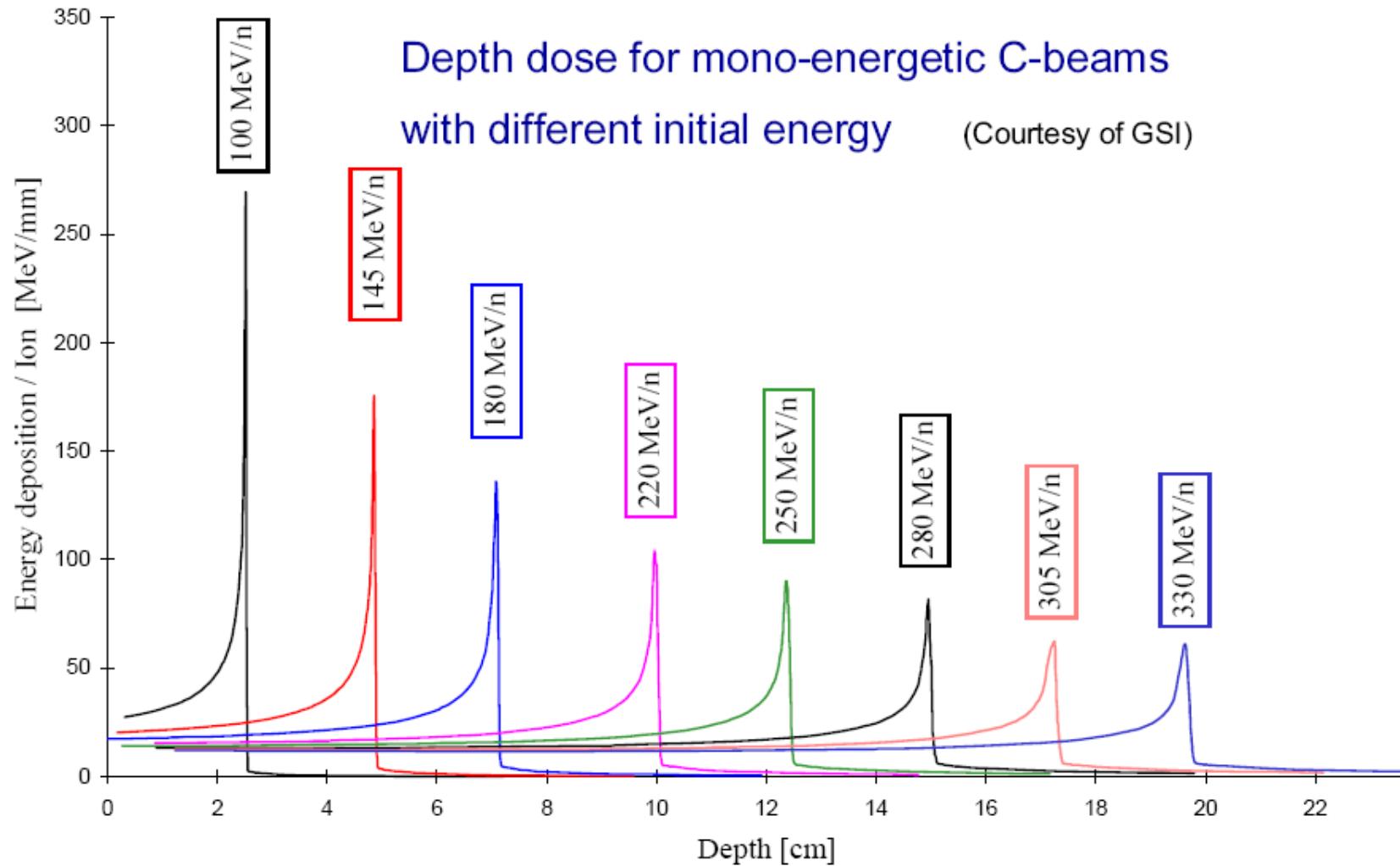
$$-\frac{dE(x)}{dx} \propto \frac{1}{v(x)^2}$$

Maximum at end of track ($v \rightarrow 0$)



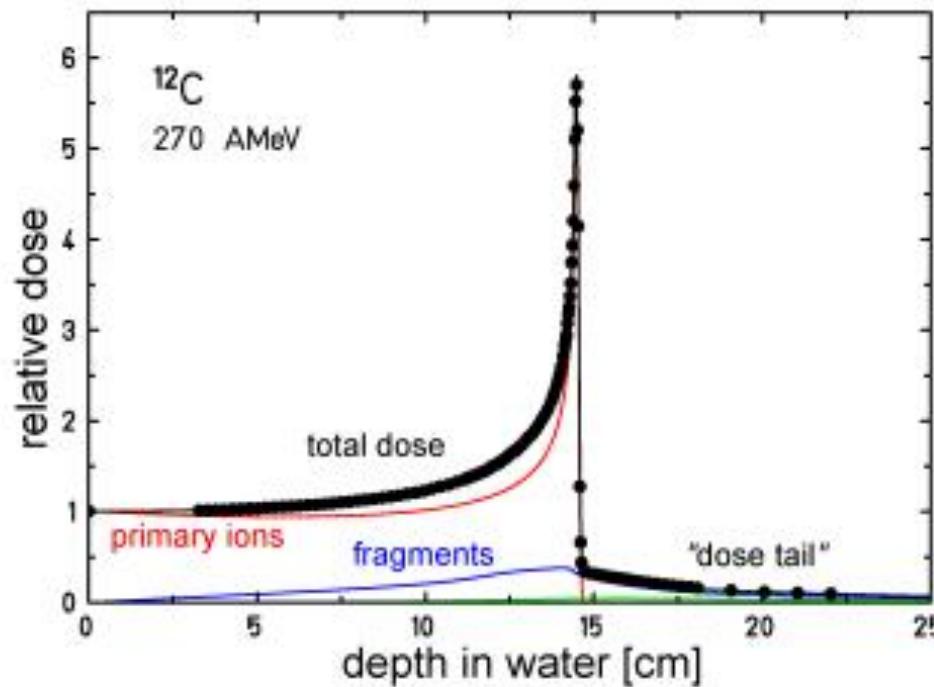
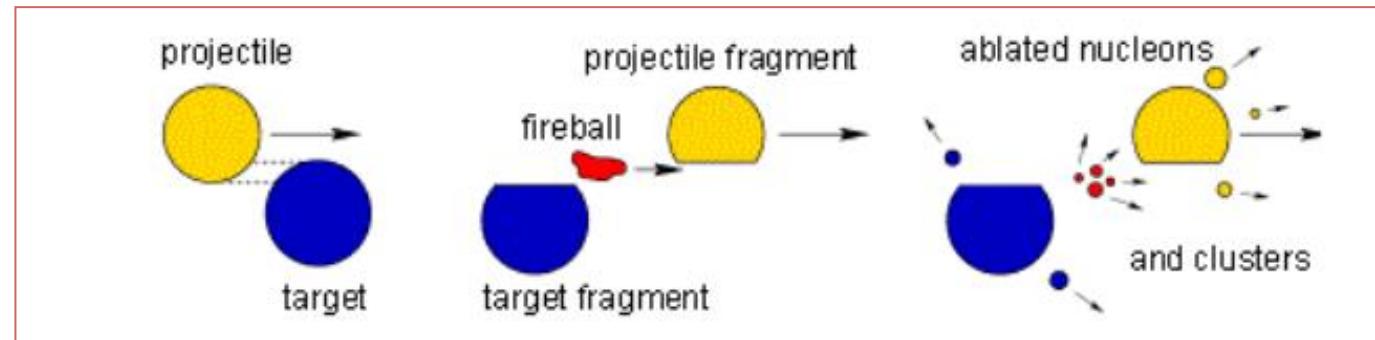
Proton Beam Therapy – Energy deposit

Energy dependence of the Bragg peak



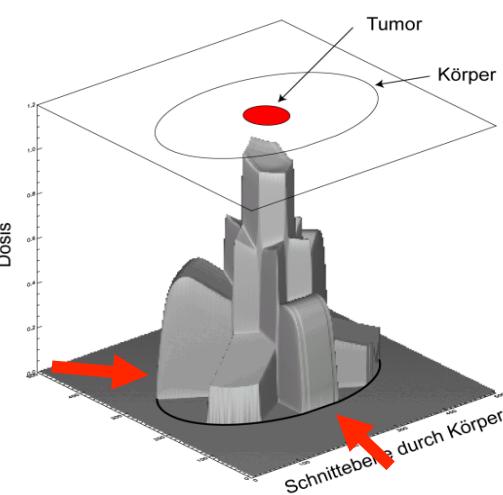
Proton Beam Therapy – Energy deposit

Fragmentation: Nuclear reactions in the tissue

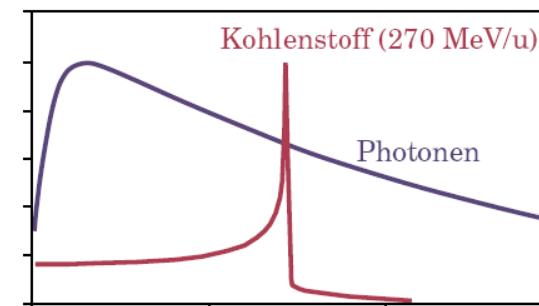
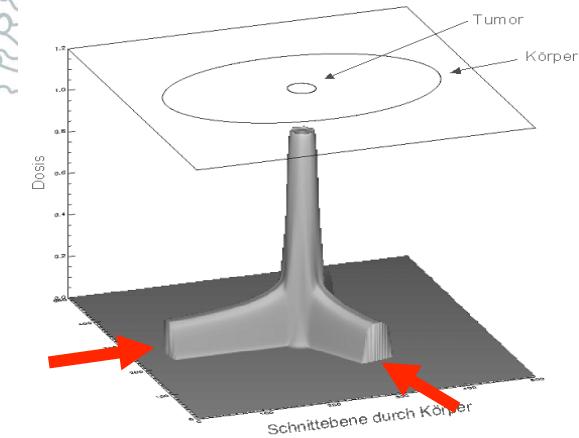


Proton Beam Therapy – Energy deposit

Photons



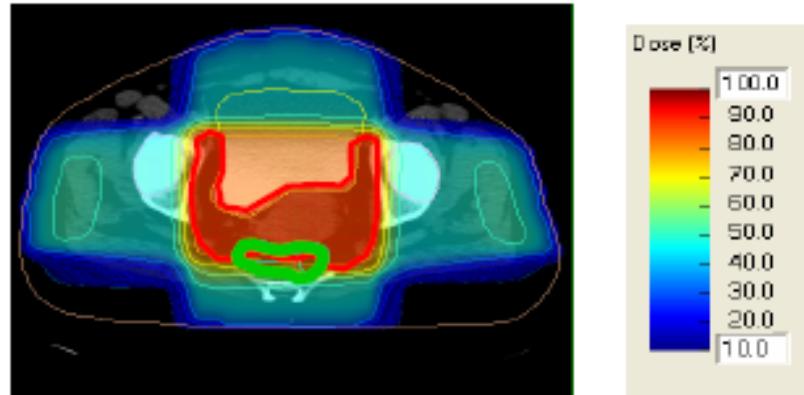
Charged particles



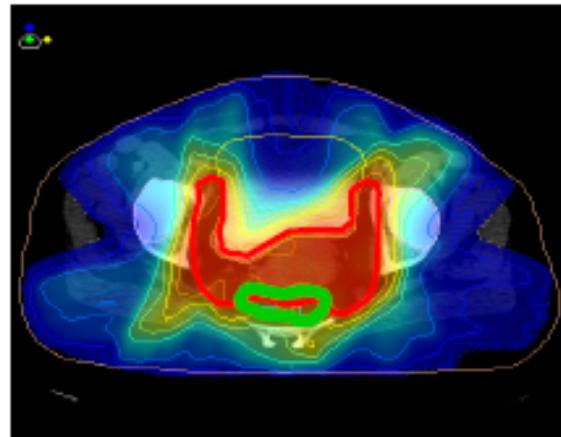
Proton Beam Therapy – Energy deposit

Simulation for irradiation at cervical

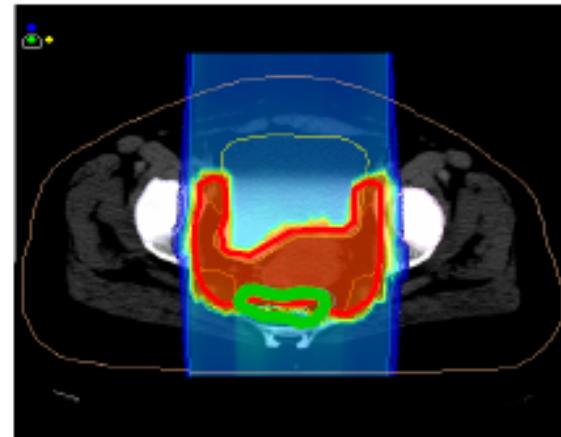
Conformal RT 4 fields



IMRT 7 fields

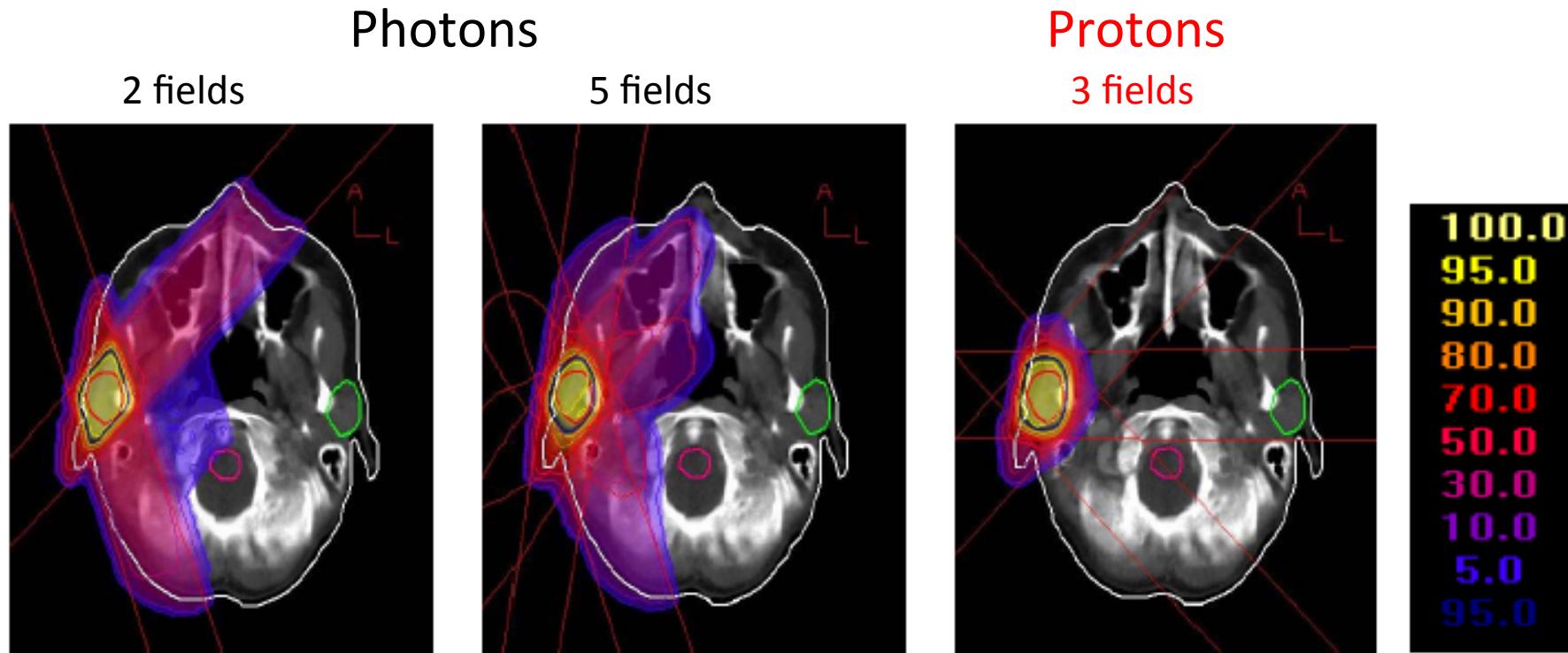


Protons 2 fields



Proton Beam Therapy – Energy deposit

Simulation for irradiation of brain



Universitätsklinik für Strahlentherapie und Strahlenbiologie, AKH, Wien

Better dose distributions with Protons

Proton Beam Therapy – Units

Activity

Number of times each second a radioactive material decays and releases radiation

Dose (Absorbed)

Amount of radiation energy absorbed into a given mass of tissue

Dose (Equivalent)

Energy per unit mass times adjustments for the type of radiation involved (quality factor) and the biological response in the tissue (a weighting factor)

Equivalent dose converts dose into a measure of risk

Proton Beam Therapy – Units

Activity

1 decay/second = 1 Becquerel (Bq)

Dose (Absorbed)

1 Joule/kg = 1 Gray (Gy)

Dose (Equivalent)

1 Gray x quality factors = 1 Sievert (Sv)

Proton Beam Therapy – Units

Radiation Weighting Factors

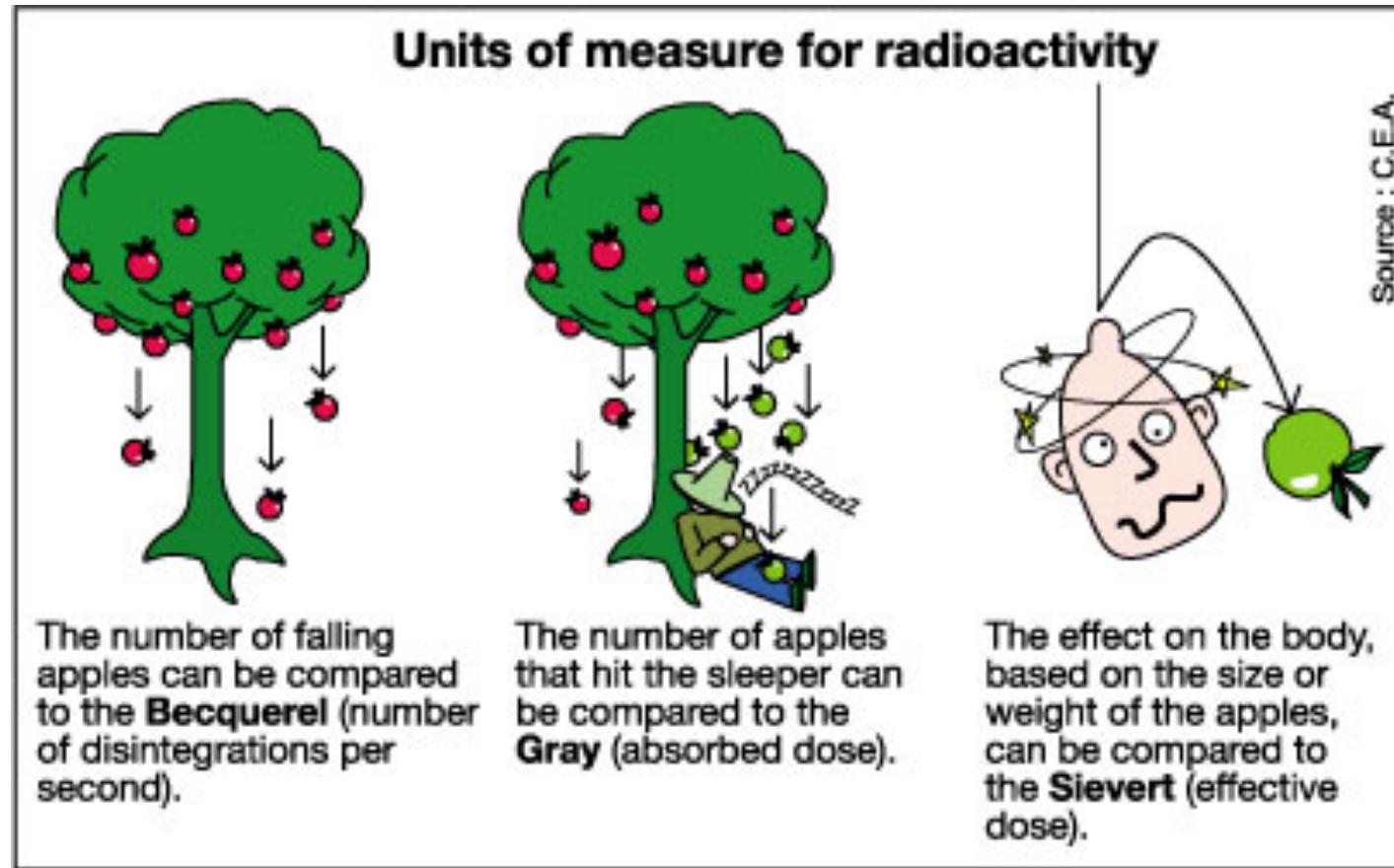
Type and Energy Range	Weighting Factor
X and γ rays, electrons, positrons and muons	1
Neutrons <10 keV	5
Neutrons 10 keV to 100 keV	10
Neutrons 100 keV to 2 MeV	20
Neutrons 2 MeV to 20 MeV	10
Neutrons >20 MeV	5
Protons, other than recoil protons and energy >2 MeV	2
Alpha particles, fission fragments, nonrelativistic heavy nuclei	20

Proton Beam Therapy – Units

Tissue Weighting Factors

0.01	0.05	0.12	0.20
Bone surface	Bladder	Bone Marrow	Gonads
Skin	Breast	Colon	
	Liver	Lung	
	Esophagus	Stomach	
	Thyroid		
	Remainder		

Proton Beam Therapy – Units



Typical doses

course of therapy	60 Gy (6000 cGy = 6000 rads)
whole body LD ₅₀	4.5 Gy (450 cGy = 450 rads)
rad. worker limit (annual)	0.05 Sv (50 mSv = 5 rems) *
non-rad. worker (annual)	0.005 Sv (5 mSv = 0.5 rems)
general public limit (annual)	0.0005 Sv (0.5 mSv = 0.05 rems)
natural background (annual)	~0.003 Sv (3 mSv = 0.3 rems)
diagnostic chest x-ray	~0.00007 Sv (70 µSv = 7 mrem)
5 hour jet flight	~0.00003 Sv (30 µSv = 3 mrem)
dental x-ray	~0.00002 Sv (20 µSv = 2 mrem)

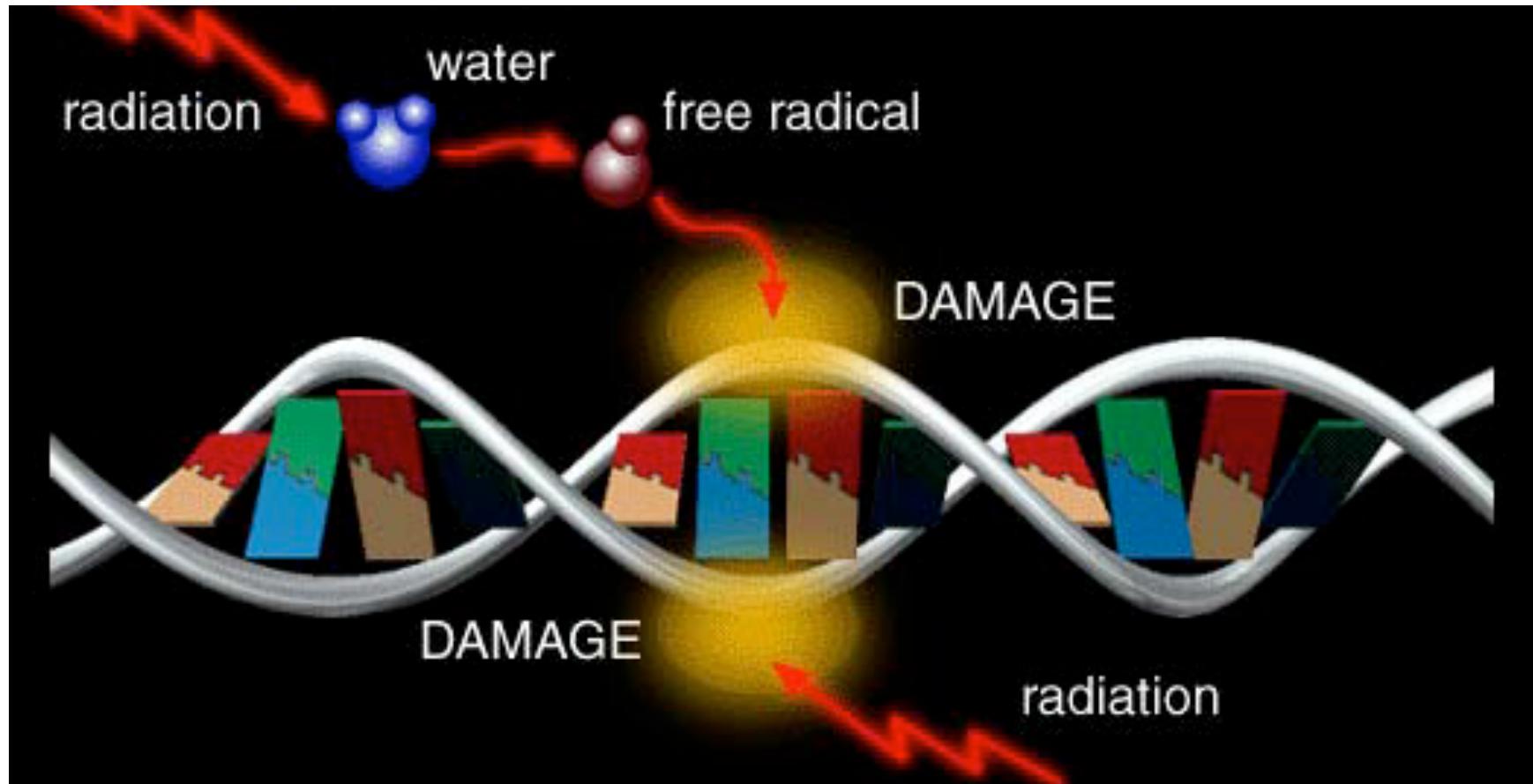
Proton Beam Therapy – Units

Lethal dose: 4.5 Gy (LD_{50}) for a man of 70 kg

$$\text{Energy absorbed} = 4.5 \text{ Gy} \times 70 \text{ kg} \approx 300 \text{ J}$$

Thermal energy content of a sip of hot coffee if derived in the form of X-rays can be lethal

Proton Beam Therapy – Biological effects



Proton Beam Therapy – Biological effects

DNA double-strand breaks increase biological effectiveness

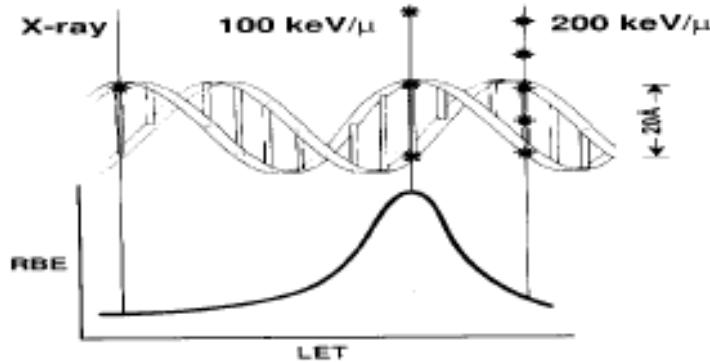
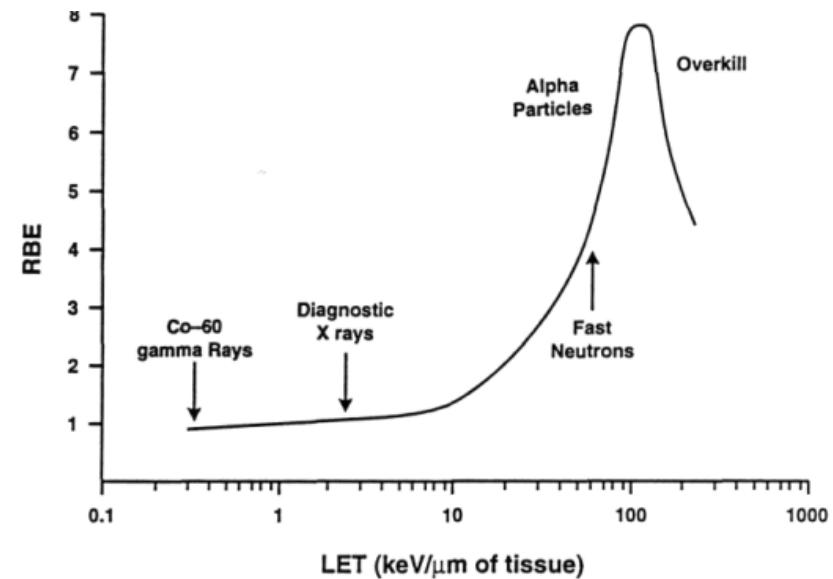
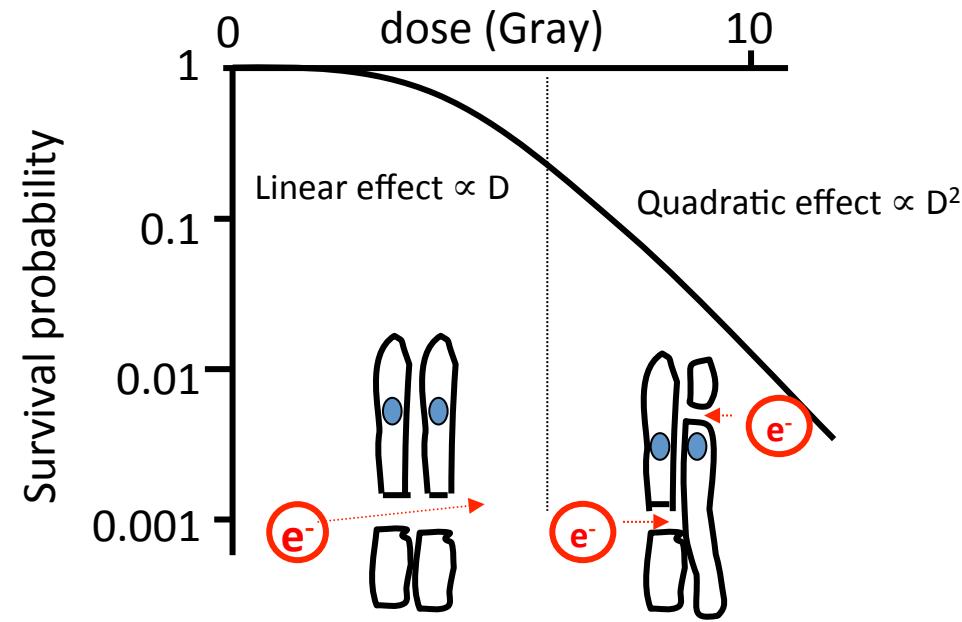


Figure 9-7. Diagram illustrating why radiation with an LET of 100 keV/ μ m has the greatest RBE for cell killing, mutagenesis, or oncogenic transformation. For this LET, the average separation between ionizing events coincides with the diameter of the DNA double helix (ie, about 20 Å [2 nm]). Radiation of this quality is most likely to produce a double-strand break from one track for a given absorbed dose.



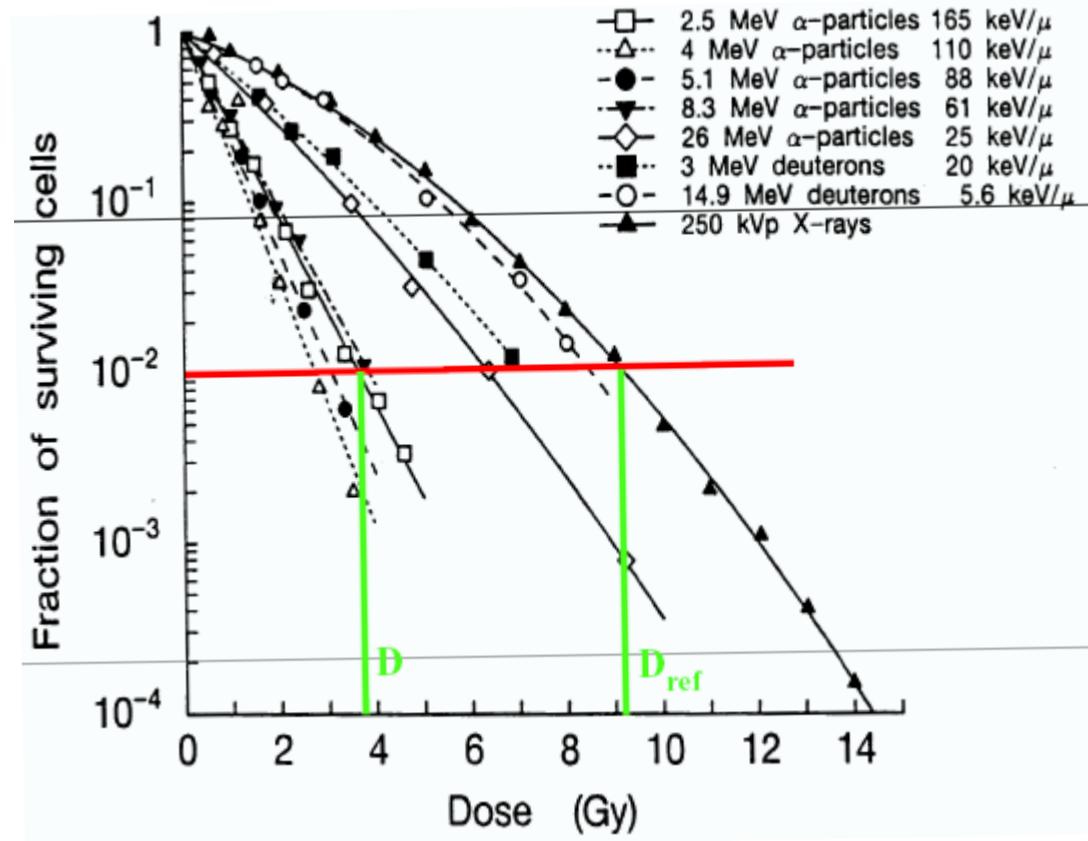
Proton Beam Therapy – Biological effects



$$\text{effect} \propto \alpha \cdot D + \beta \cdot D^2$$

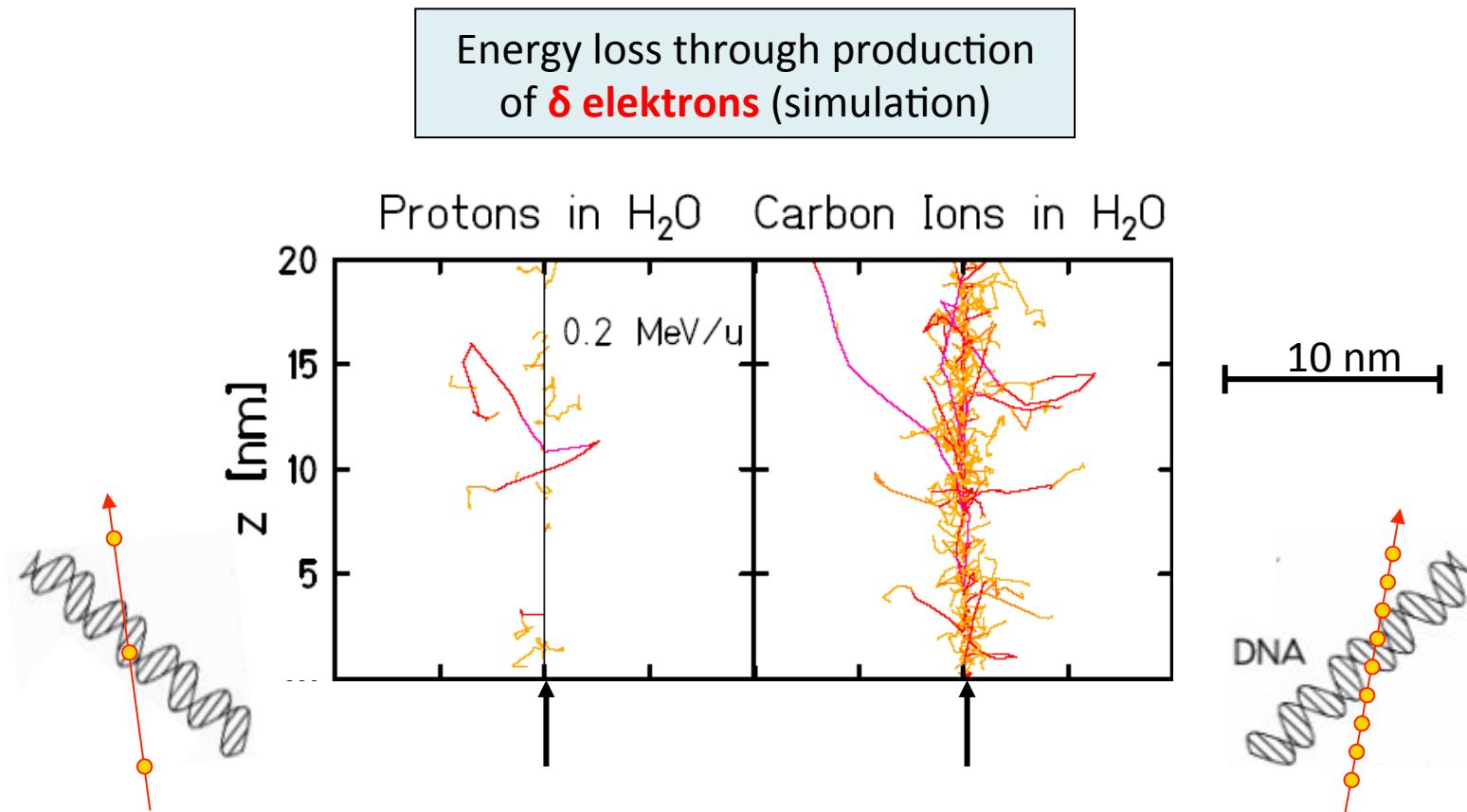
Relative biological effectiveness (RBE)

$$RBE = \frac{\text{Dose of reference radiation with effect } X}{\text{Dose of radiation of interest with effect } X}$$



Proton Beam Therapy – Protons vs. Ions

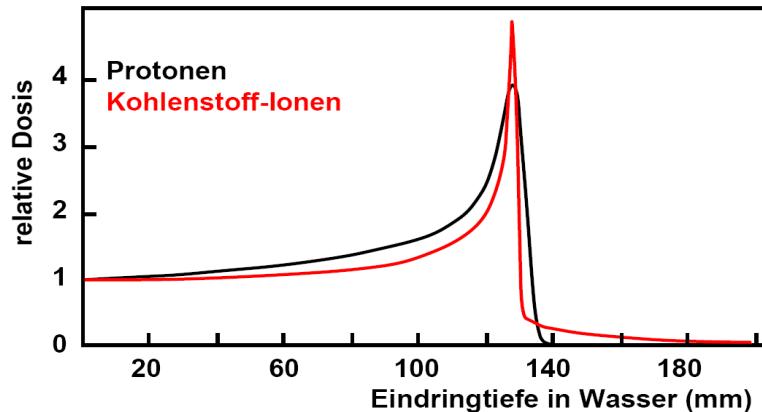
Increased biological effectiveness



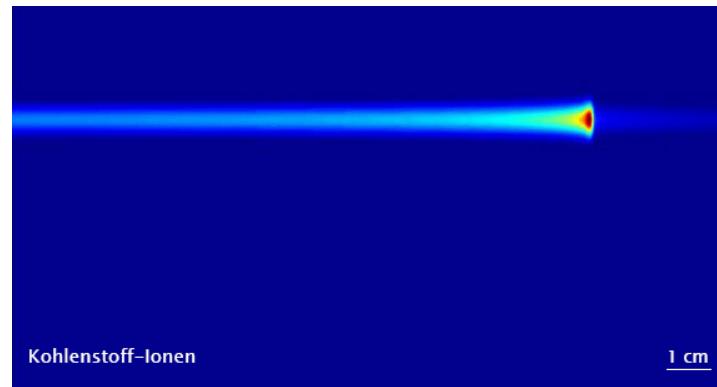
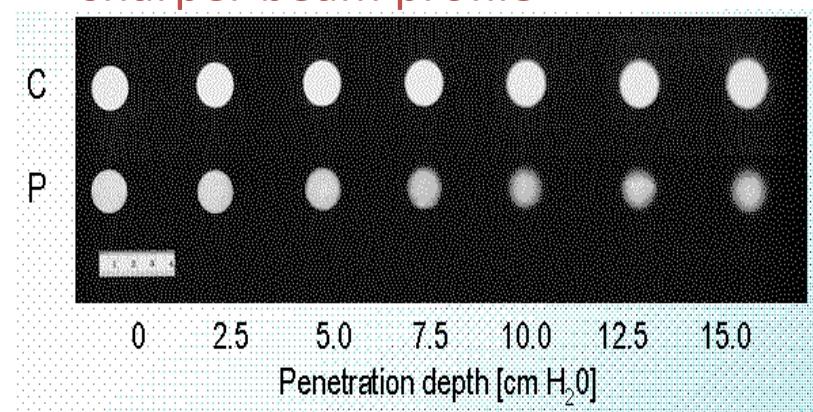
Proton Beam Therapy – Protons vs. Ions

Extremely localized energy loss

Longitudinally
narrower Bragg-Peak



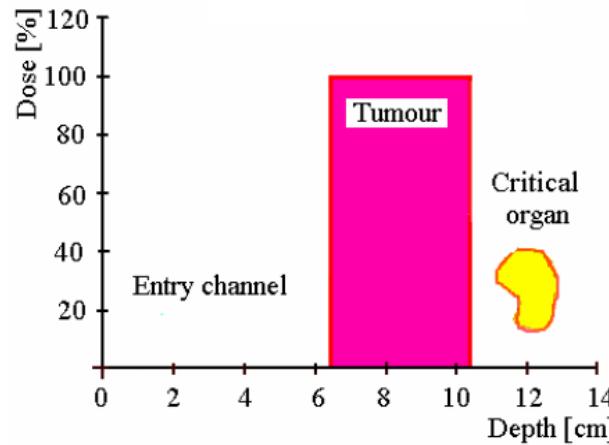
Transversally
sharper beam profile



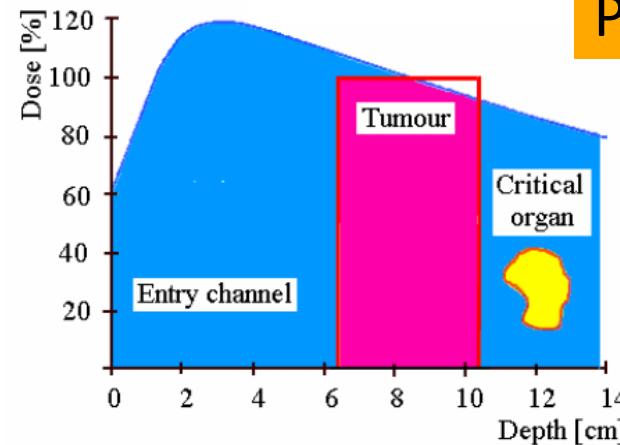
Proton Beam Therapy – Protons vs. Ions

Dose distributions

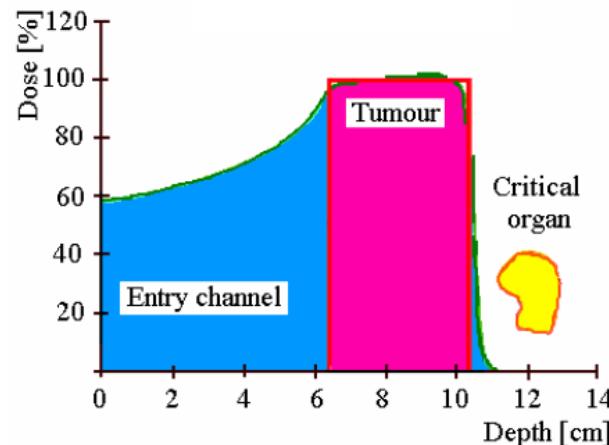
Ideal



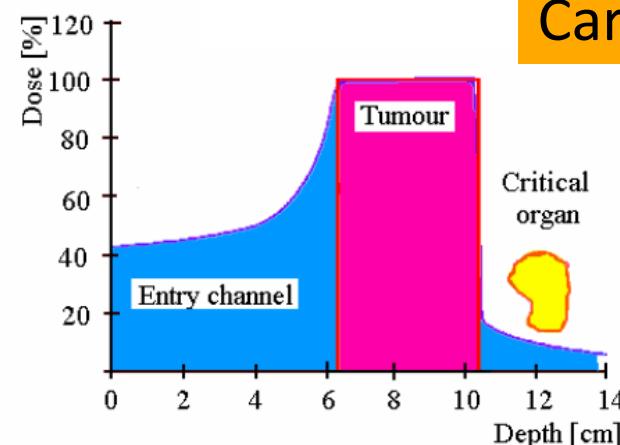
Photons



Protons



Carbon

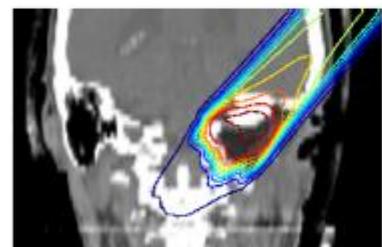
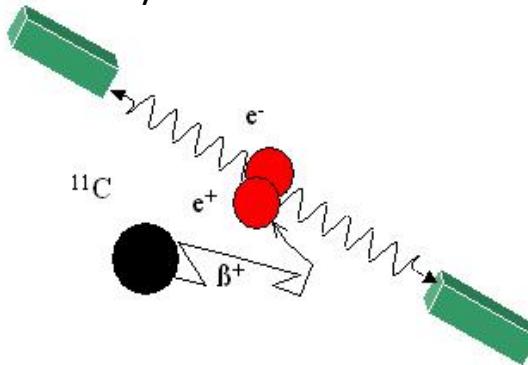


Proton Beam Therapy – Protons vs. Ions

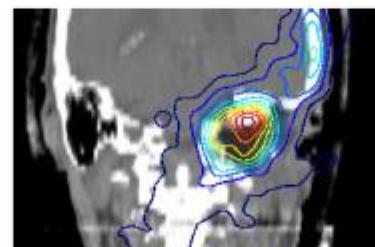
PET Diagnostics

Fragmentation of ^{12}C → Positron emitting isotopes

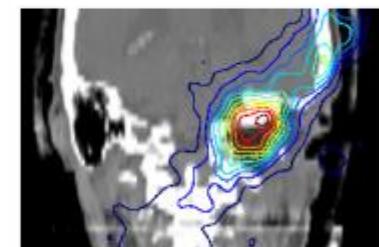
^{11}C ($T_{1/2} = 20 \text{ min}$), ^{10}C ($T_{1/2} = 19 \text{ s}$), ...



planned physical
dose distribution



PET measured
positron emitters

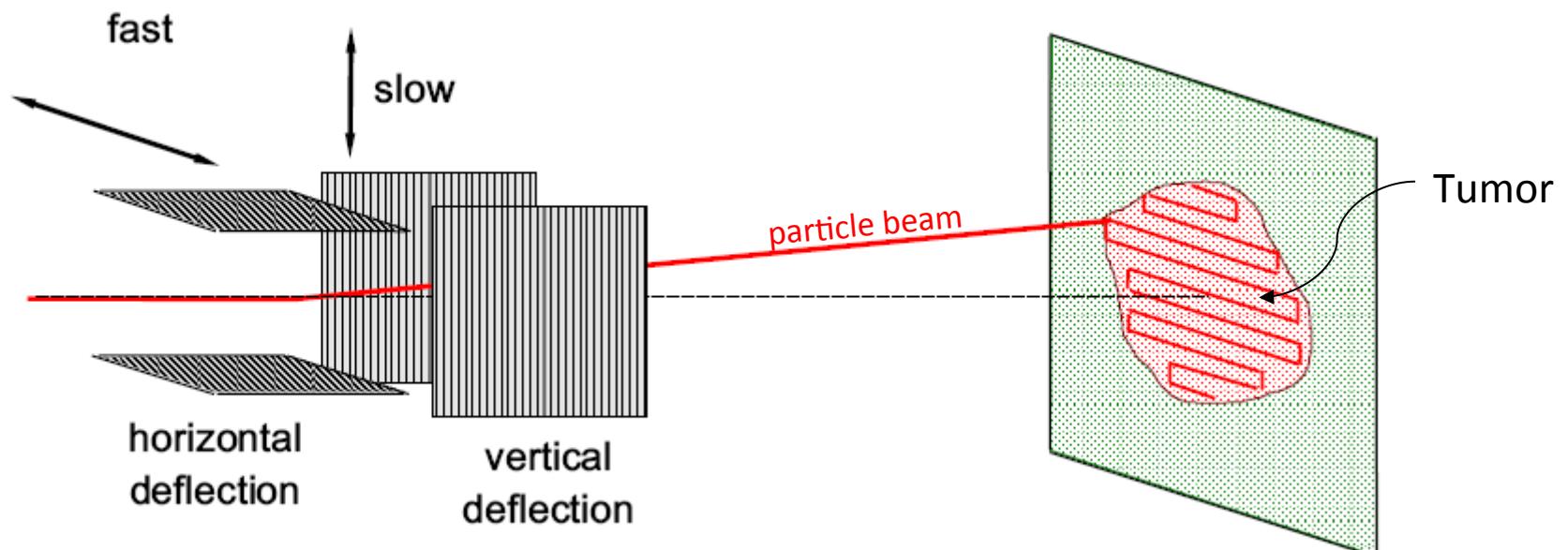


PET simulated
positron emitters

Lateral resolution
ca. 2.5 mm

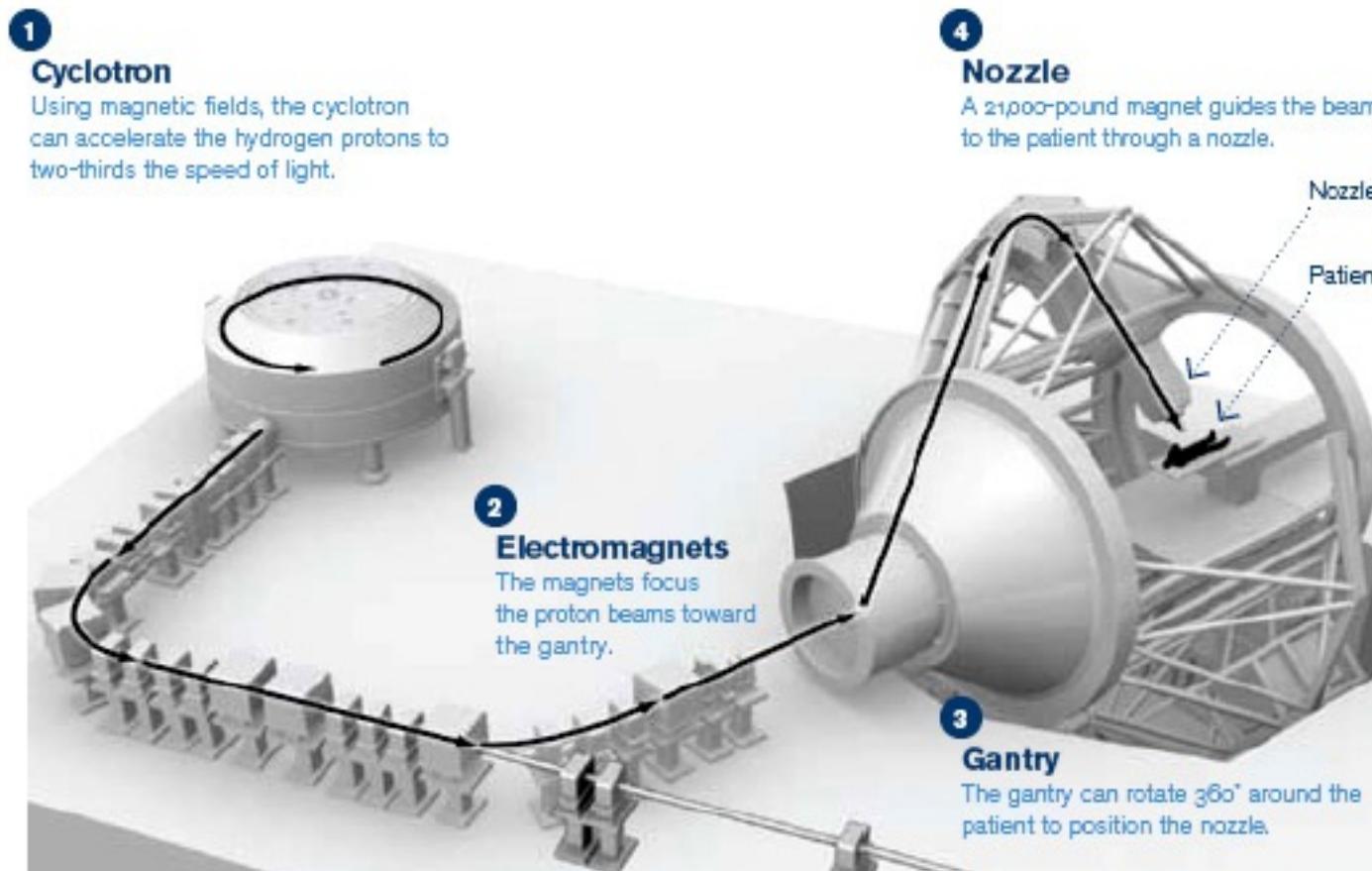
Proton Beam Therapy – 3d treatment

2d scanning & energy variation = 3d



Proton Beam Therapy – 3d treatment

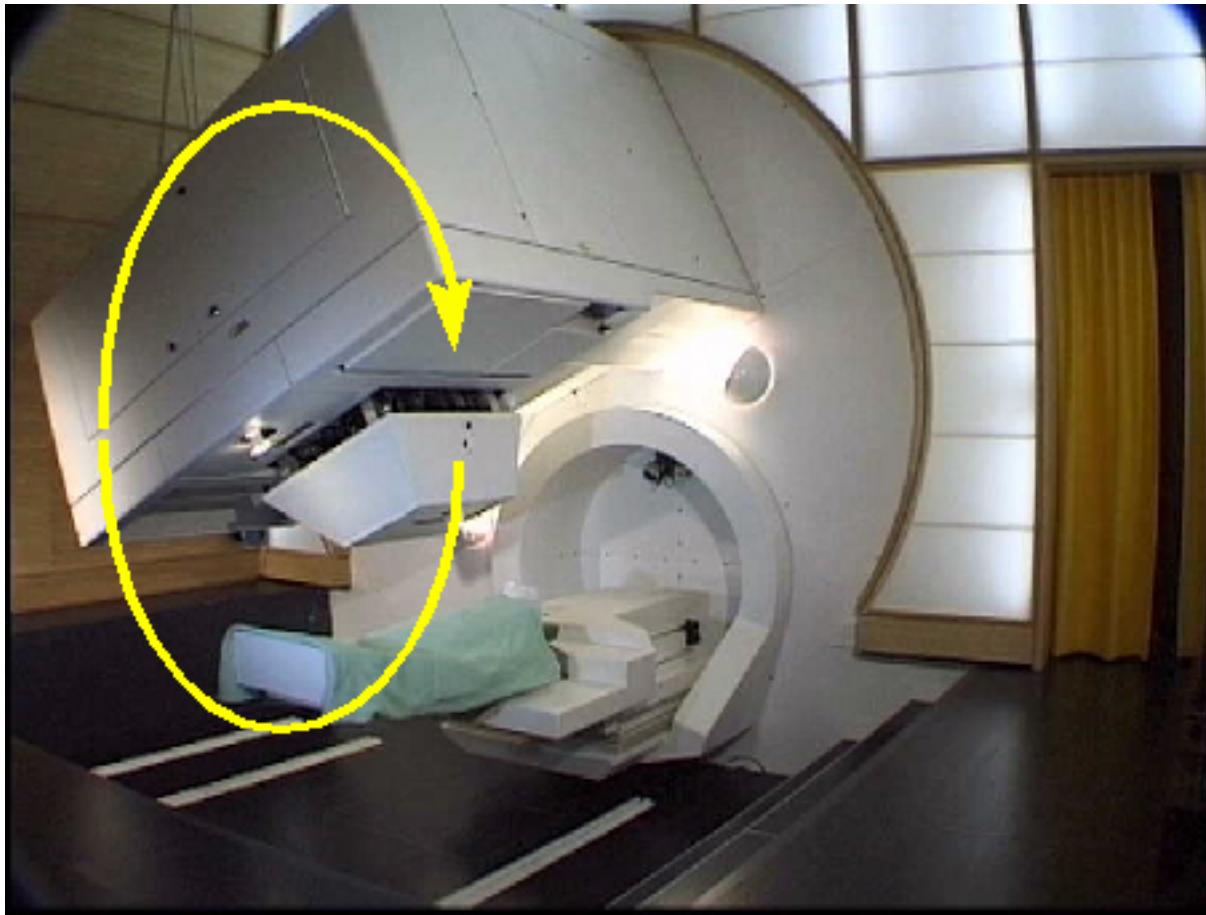
Gantries: allow for irradiation from all sides



The Israel Proton Therapy Initiative

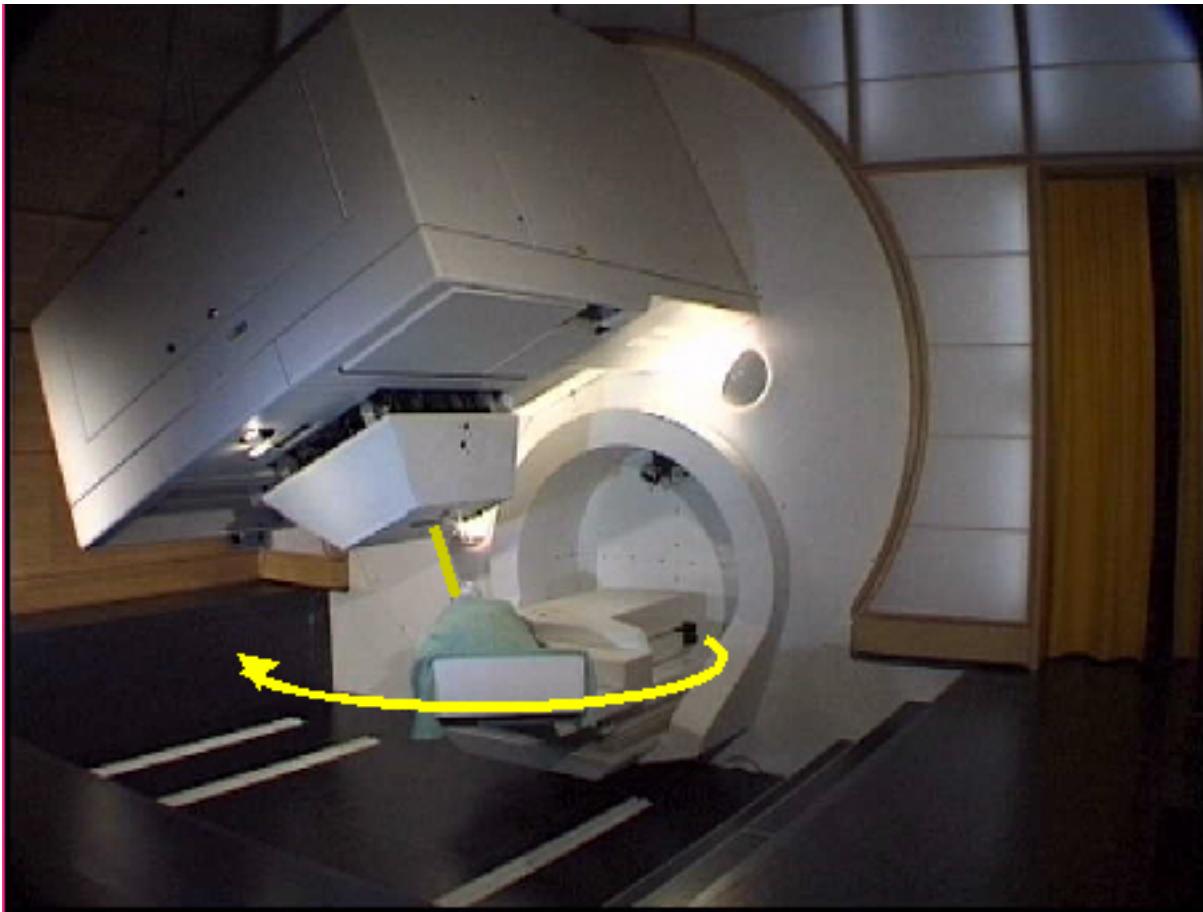
Proton Beam Therapy – 3d treatment

Gantry at PSI Villigen (Switzerland)



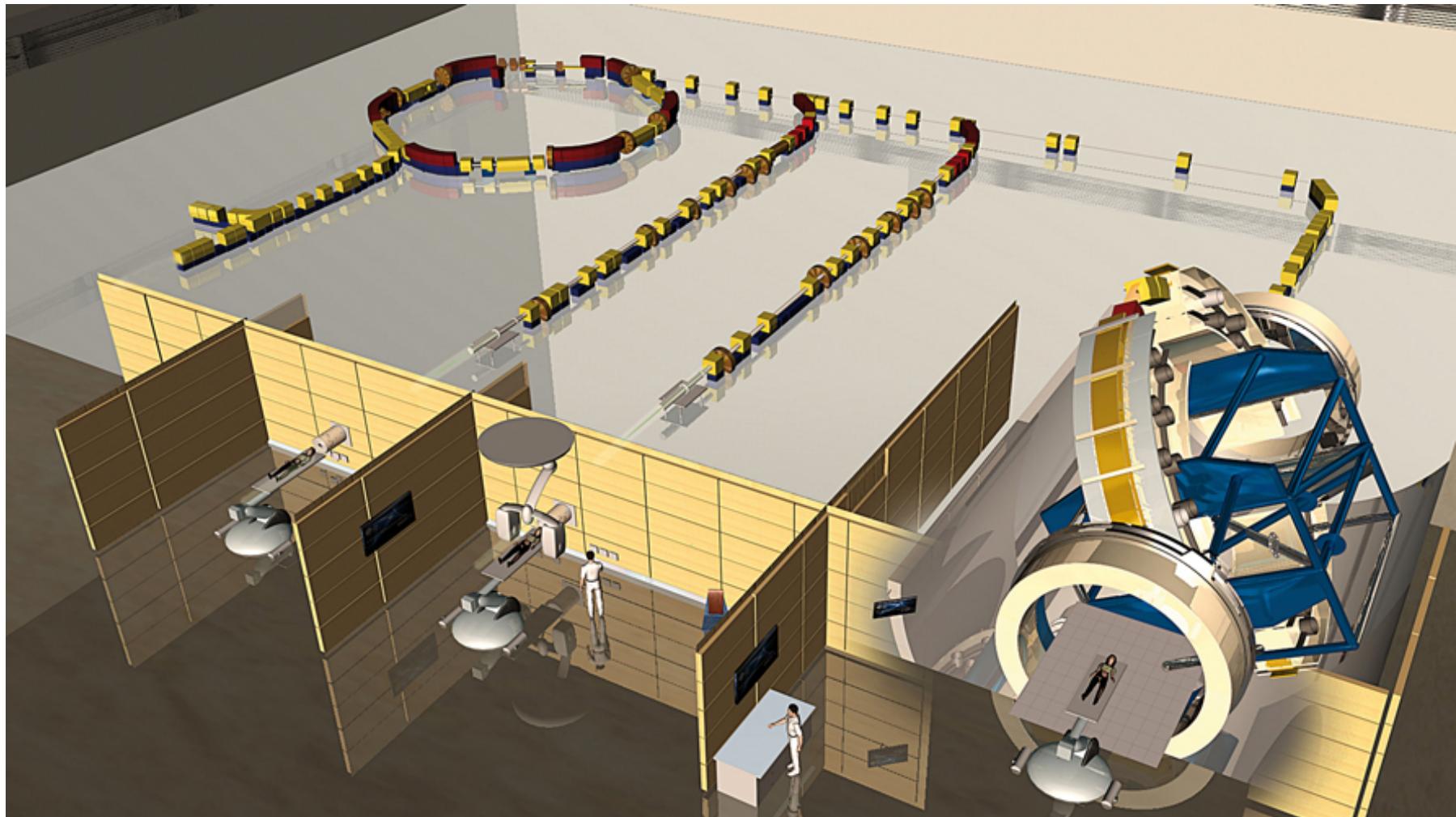
Proton Beam Therapy – 3d treatment

Gantry at PSI Villigen (Switzerland)



Proton Beam Therapy – Facilities

HIT (Heidelberg)



Proton Beam Therapy – Facilities

HIT (Heidelberg)

Proton Beam Therapy – Treatment

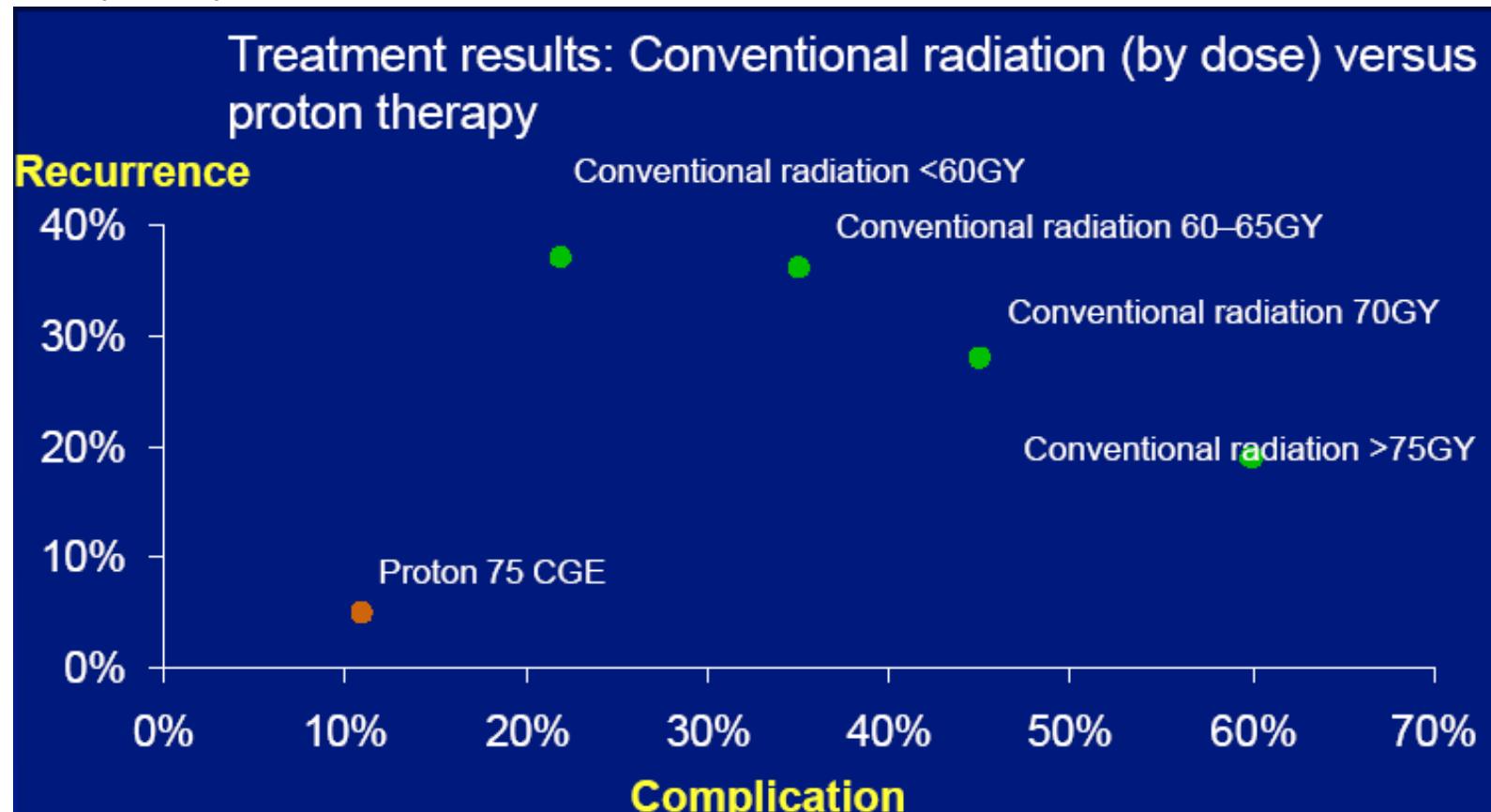
Research facility at GSI Darmstadt (1997 – 2008)

- over 180 patients (07/2003)
- approx. 70 % ^{12}C , 30 % ^{12}C + photons
- 350 days of clinical operation
- typical parameters:
 - approx. 20 fractions per patient
 - 2-4 fields per fraction
 - 3-3,5 Gye per fraction
 - tumor volumes: 50-3200 cm³
 - 1000-45000 points per tumor
 - 2-12 min. per field
- no in-field recurrence (2 out-of-field)
- only very mild side effects
- partially accepted as curative method



Proton Beam Therapy – Treatment

Treatment of prostate cancer at Loma Linda University Medical Center (USA)

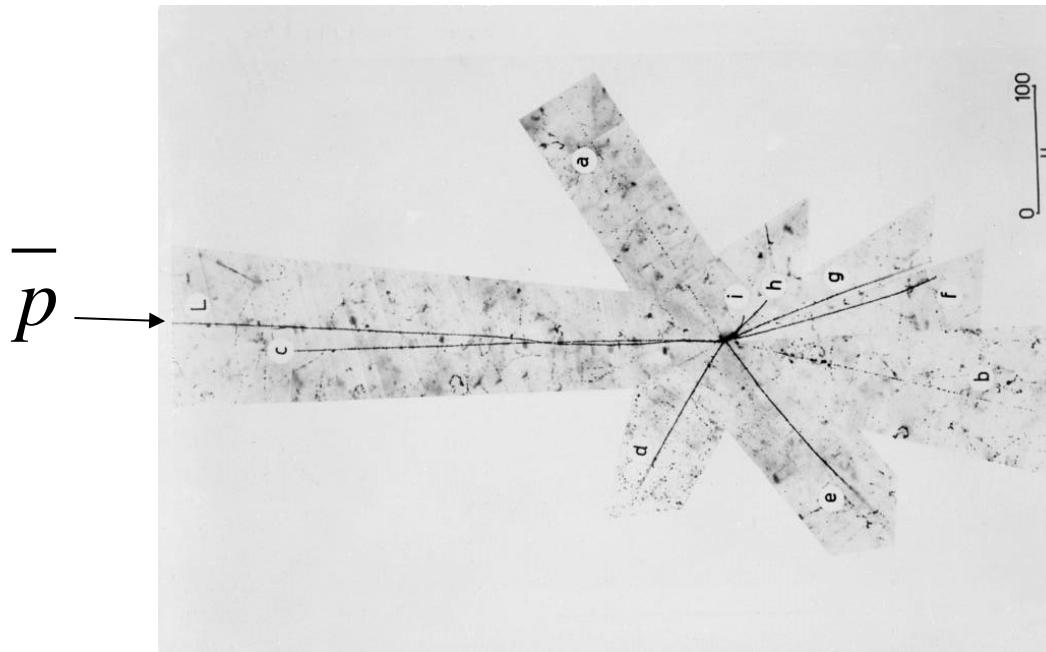


No double blind studies yet!

Proton Beam Therapy – The future

Irradiation with Antiprotons???

In principle, Antiprotons deliver an energy of $E = 2m_p c^2 \sim 2000$ MeV besides their kinetic energy (~ 100 MeV)



First observation of a Proton-Antiproton annihilation (1955)

Proton Beam Therapy – The future

Laser-induced particle acceleration

